

### Wound Healing Composition

The present invention relates to compositions and methods for tissue regeneration, particularly for treating skin lesions such as wounds. The compositions and methods are useful especially for assisting the process of wound healing, particularly chronic open lesions that are slow to heal or resistant to healing.

Healing of open wounds extending through the germinal epithelium in otherwise healthy tissue takes place by the process classically described as “second intention”, which, following initial haemostasis, involves a well-ordered sequence of inflammation, cellular infiltration, angiogenesis, granulation and re-epithelialisation. As part of the normal healing response, resident fibroblasts are required to undergo a series of phenotypic changes, migrating to the wound site, then proliferating, then synthesising and secreting extracellular matrix molecules. *In vivo*, at least a proportion of fibroblasts then switch to a myofibroblastic phenotype in order to facilitate wound contraction.

*In vitro*, a series of phenotypically distinguishable mitotic and post-mitotic fibroblast populations have been described (Bayreuther *et al.*, 1988, Proc Natl Acad Sci USA 85: 5112–5116). The pathway of differentiation appears to be controlled, at least in part, by interactions between fibroblasts and extracellular matrix (ECM) proteins present at the wound site. Growth factors and cytokines undoubtedly also exert an important influence, although their effects too, appear to be modulated by fibroblast exposure to particular ECM proteins. Among the ECM proteins that appear to have an important role in fibroblast differentiation are fibrinogen and fibrin. Fibroblasts specifically interact with fibrin and fibrinogen “RGD” motifs through  $\alpha_v\beta_3$  integrin receptors although the cellular response is complex and modulated by other factors. *In vitro* studies of the effect of fibrin glue on human periodontal ligament fibroblasts have suggested that fibrin appeared to slightly inhibit fibroblast proliferation. The presence of a fibrin matrix has also been reported to increase the synthesis of collagen by

entrapped fibroblasts (Neidert *et al.*, 2001, Proceedings of the ASME Bioengineering Conference, Kamm *et al.* [Eds], Vol 50: 215–216).

5 Fibroblasts are also known to have a role in the remodelling of fibrin clots. As new extracellular matrix proteins such as collagen type I and III, fibronectin and vitronectin are laid down, the fibrin matrix is broken down, predominantly by the activation of the plasma-derived enzyme plasmin. This is regulated by the activation (or inhibition) of its proenzyme, plasminogen, by a variety of plasminogen activators and inhibitors. *In vivo*, a number of infiltrating cells, 10 such as neutrophils and macrophages, secrete urokinase-type plasminogen activator (uPA), whilst endothelial cells are largely responsible for producing tissue plasminogen activator (tPA). Fibroblasts also secrete both uPA and plasminogen activator inhibitors, such as plasminogen activator inhibitor-1 (PAI-1). The balance between these antagonistic mediators is crucial in controlling 15 fibrin remodelling and scar formation. The expression of the antagonistic mediators is developmentally regulated, as well as being controlled by extracellular matrix components and local growth factors.

To facilitate movement through a cross-linked fibrin clot and a tight meshwork 20 of extracellular matrix, a variety of fibroblast- and serum-derived enzymes cleave a path for migration. These include interstitial collagenase (matrix metalloproteinase-1, MMP-1), gelatinase (matrix metalloproteinase-2, MMP-2), stromelysin (matrix metalloproteinase-3, MMP-3) and the plasminogen activators. Chemotactic factors such as TGF- $\beta$  and PDGF may upregulate the 25 production and secretion of these enzymes.

Once migrating fibroblasts reach a wound, they gradually become secretory and protein synthesis is increased. The previously retracted endoplasmic reticulum and Golgi apparatus becomes dispersed throughout the cytoplasm and a loose 30 matrix is produced, which is mainly composed of fibronectin and type III collagen. Ultimately, this profibrotic phenotype takes over, which is characterised by an abundance of rough endoplasmic reticulum and Golgi

apparatus, secreting newly synthesised collagen in response to highly expressed TGF- $\beta$ . Notwithstanding, TGF- $\beta$  fails to upregulate further collagen deposition, once a matrix has been deposited. It is also thought that IL-4 released by mast cells induces a modest increase in types I and III collagen together with  
5 fibronectin. Mast cells furthermore produce tryptase (a serine esterase) in abundance, which has been shown to upregulate fibroblast proliferation.

Stimuli such as TGF- $\alpha$ , TGF- $\beta$  and PDGF responsible for fibroblast proliferation and matrix synthesis have been extensively investigated *in vitro*  
10 (Derynck, 1988, Cell 54: 593-595; Ross & Raines, 1990, In: Growth Factors: From genes to clinical applications, Sara *et al.* [Eds], pp. 193-199, Raven Press, New York; Sporn & Roberts, 1992, J Cell Biol 119: 1017-1021) and by *in vivo* manipulation of wounds (Sprugel *et al.*, 1987, Am J Pathol 129: 601-613; Pierce *et al.*, 1991, J Cell Biochem 45: 319-326).  $\gamma$ -interferon on the other hand  
15 was demonstrated to have a negative effect on the mitogenic and synthetic potential of fibroblasts *in vitro* and *in vivo* (Duncan & Berman, 1985, J Exp Med 162: 516-527; Granstein *et al.*, 1987, J Clin Invest 79: 1254-1258). In addition, the collagen matrix itself can suppress these activities (Grinnell, 1994, J Cell Biol 124: 401-404; Clark *et al.*, 1995, J Cell Sci 108: 1251-1261), whilst  
20 fibrin or fibronectin matrix have little or no suppressive effect (Clark *et al.*, 1995, *supra*). Many fibroblasts undergo apoptosis (programmed cell death) in day-10 healing wounds, thereby marking the transition from a fibroblast-rich granulation tissue to a scar tissue with reduced cell density.

25 Where a wound has destroyed the germinal layer of epithelium, collagen deposition by infiltrating fibroblasts and re-epithelialisation results in a degree of scarring, with incomplete restoration of function in terms of the flexibility and elasticity of the original dermis and failure to regenerate auxiliary structures such as hair follicles and sweat glands.

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A number of factors may adversely affect the rate and extent of such wound healing, in particular, poor blood supply. Poorly perfused tissue, often

associated with impaired venous return and varicose veins, peripheral vascular disease or diabetes, often fails to heal satisfactorily, resulting in chronic ulcers, although the details of the pathogenesis are still unclear. Chronic leg ulcers in particular are a significant and growing problem world-wide.

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Various approaches have been tried for the treatment of wounds. Autologous skin-grafting has been used to close open wounds, minimise the risk of opportunistic infection, accelerate healing and minimise scarring. Skin grafting has significant limitations, not least the requirement for a suitable donor site from which grafts can be taken which is a particular problem where wounds are extensive (for example, with burns). In addition, grafts have a low success rate where wound healing is compromised.

With respect to chronic leg ulcers in particular, the introduction of compression therapy in combination with moist wound dressings has been the standard therapeutic management.

More recently, tissue-engineering solutions have become available. Research into regenerative medicine has shown that human cells have substantial potential to heal and regenerate damaged tissue especially when primed by an environment that closely mimics the natural physiological condition being treated. Much of this research has focused on the production of so-called "tissue equivalents", which aim to provide a temporary functional replacement for missing tissue and accelerate healing. Tissue equivalents may be dermal equivalents or total skin equivalents, with the aim being to provide effective coverage of the wound as quickly as possible. The development and production of tissue equivalents usually involves the isolation of replacement skin cells, which are expanded and seeded onto or into a supporting structure such as a three-dimensional bio-resorbable matrix, or within a gel-based scaffold.

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A variety of materials have been used as acellular protein matrices for wound healing applications. These include synthetic polyesters (polyglycolic acid

(PGA), polylactic acid (PLA), polyglactide (Dermagraft [RTM], Smith & Nephew, described below), polydioxanone, polyhydroxyalkanoates and hyaluronic acid derivatives), hydrophilic polyurethanes (polyetherpolyester, polyethylene oxide and carboxymethylcellulose ethylene), and collagen-based  
5 scaffolds (cross-linked elastin collagen material (Matriderm [RTM]), cross-linked collagens manufactured from acid-soluble type I bovine collagen material (such as Vitaphore [RTM]). An alternative approach is to use an acellular derivative of allogeneic human dermis, a natural dermal matrix from which cells have been removed (such as Alloderm [RTM], LifeCell  
10 Corporation). Some preparations use an organised, layered structure in order to more closely mimic the structure and function of the dermis. For instance, a preparation comprising an underlying layer of bovine collagen and shark glycosaminoglycans with an overlying layer of silicone is known (Integra [RTM], Integra LifeSciences Corporation).

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Other approaches to wound healing have involved the use of fibrin sealants, for example Tisseel [RTM] (Baxter), Beriplast [RTM] (Aventis), Quixil [RTM] (Omrix Biopharmaceuticals), Haemaseel [RTM] (Haemacure) and Crosseal [RTM] (Omrix). These commercially available fibrin sealants are derived from  
20 cryoprecipitate of pooled plasma from virally-screened allogeneic donors.

Fibrin products rely on the natural polymerisation process that occurs during the physiological blood clotting cascade, in which a monomeric fibrin precursor, fibrinogen, is acted on by activated thrombin with the resultant production of  
25 polymeric fibrin. Fibrin forms the protein scaffold component of blood clots, to which platelets adhere.

Fibrin has been recognised as a convenient and clinically acceptable cell carrier to be used in tissue engineering applications. Commercially available products  
30 that utilise fibrin sealants for cell delivery include Bioseed [RTM] (Biotissue Technologies). The use of fibrin sealants for cell delivery purposes for the treatment burns has been suggested by several groups (see Brown *et al.*, 1993,

Am J Pathol 142: 273–283; Neidert *et al.*, 2001, *supra*; Tuan *et al.*, 1996, Exp Cell Res 223: 127–134; and US Patent Appl. No. 2003/01654482).

5 Exogenously applied dermal cells have been shown to have beneficial effects on wound healing including shorter time to complete healing (Falanga & Sabolinski, 1999, Wound Repair Regen 7: 210–207), delivery of active growth factors to the wound (Naughton *et al.*, 1997, Artif Organs 21: 1203–1210), reduced potential for lesion recurrence (Gentzkow *et al.*, 1996, Diabetes Care 19: 350–354), and reduced pain (Muhart *et al.*, 1999, Arch Dermatol 135: 913–  
10 918).

Known combinations of protein matrices and dermal cells for wound healing applications include a preparation called Dermagraft [RTM] (Smith & Nephew) comprising cryo-preserved primary human foreskin fibroblasts seeded onto a  
15 bioabsorbable glycolic-lactic acid polyester (polyglactide) scaffold (Naughton *et al.*, 1997, *supra*; US4,963,489). The fibroblasts are allowed to proliferate in the scaffold, secreting extracellular matrix proteins and growth factors and cytokines. The mature preparation is packaged in 10% dimethylsulphoxide and bovine serum as a cryoprotectant to allow storage of the product by freezing  
20 prior to use. Disadvantages of this approach include difficulty in manipulating the product during application to the wound (such as ulcers), and the necessity of storing and transporting the product at very low temperatures (-70°C) and use of careful thawing procedures in order to ensure viability of the cells (see WO 87/06120).

25 Various combinations of collagen-based matrices and living cells are known. Apligraf [RTM] (Organogenesis, Inc.) is a bilayered structure comprising a lower ('dermal') layer of a bovine collagen scaffold supporting living human fibroblasts and an upper ('epidermal') layer comprising human keratinocytes on  
30 a collagen scaffold (Falanga & Sabolinski, 1999, *supra*; WO 99/63051). The preparation is supplied as a circular disk approximately 75 mm in diameter and 0.75 mm thick on an inert polycarbonate membrane. Apligraf [RTM] is

packaged individually for use and has a 5-day shelf life. It is maintained in an agarose-rich nutrient with a 10% CO<sub>2</sub>/air atmosphere and is shipped and stored at room temperature (20°C to 31°C; 68°F to 88°F). The removal of the product from the storage dish and polycarbonate membrane involves teasing away the edge of the Apligraf [RTM] using sterile forceps. Problems associated with this method include excessive folding which can make accurate, close application of the preparation to the wound difficult and time-consuming.

A similar product (Orcel [RTM]; Ortec International Inc) is described in US6,039,760. Orcel [RTM] is a bilayered structure of bovine collagen with fibroblasts and keratinocytes. The preparation is packaged between 2 non-adherent pieces of mesh, which are differently coloured to distinguish between sides. The device is then packaged in a plastic tray containing media to maintain cell viability during storage and shipping, which is further packaged into pouches with chill packs to maintain a temperature of 11°C to 19°C for 72 hours.

Another example of a tissue equivalent that attempts to reproduce a dermis-like arrangement of fibroblasts in a protein matrix supporting an overlying layer of keratinocytes is described in Meana *et al.* (1998, Burns 24: 621–630). Rama *et al.* (2001, Transplantation 72: 1478–1485) describe a method of culturing autologous limbal stem cells on a fibrin gel substrate for grafting to the contralateral cornea.

US Patent Appl. No. 20030165482 discloses a wound healing preparation (Allox [RTM], Modex Therapeutiques SA) comprising growth-arrested allogeneic human fibroblasts and keratinocytes applied to a wound in a viscous paste of fibrinogen (Tisseel [RTM]) to which thrombin has been added, so that fibrinogen cleavage and fibrin polymerisation occur *in situ*. Alternatively, the separate liquid components are sprayed onto the wound, to set *in situ*, on mixing.

The present invention provides an alternative wound healing preparation and associated products and methods which address problems associated with prior art products and methods.

5 According to a first aspect of the present invention there is provided a wound healing composition comprising living cells within a support matrix, in which the cells have a wound healing phenotype, and in which the composition is single-layered and has been incubated for up to about 8 days to allow development of the wound healing phenotype.

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The invention provides an approach to treatment of chronic wounds based, not on providing an immediately functional tissue-equivalent, but on delivering cells, in a support matrix (which could also be referred to as a maturation matrix or a development matrix; for example a biocompatible matrix), with the potential to promote and accelerate the healing process. Although developing a viable skin equivalent (for example, a cultured dermal tissue equivalent comprising fibroblasts, extracellular matrix and overlying keratinocytes organised into functional and anatomically relevant structures) remains a worthwhile goal, so far this has proven elusive. However, for many situations, 15 the present invention shows that such an approach may be unnecessarily complex and that a simpler solution, that of providing a single layer of cells at the appropriate stage of development and exhibiting a particular phenotype in a wound-healing composition for rapid, convenient and accurate application to wounds, is remarkably effective. The cells used in the present invention develop 20 surprising rapidly to have a "wound-healing phenotype" to encourage immediate wound healing. It is believed that the wound healing phenotype represents the optimal phenotype for accelerating or assisting wound healing. The invention allows delivery of such cells (in the composition) to a wound, preferably in a manner which is consistent with the maintenance of the wound-healing phenotype. 25 30

Whether or not cells in a composition have a wound healing phenotype may be



tested by applying the composition to a wound (as defined herein) and observing whether or not healing of the wound is accelerated or assisted.

5 Wounds to which the wound healing composition may be applied include wounds such as an ulcer such as a venous ulcer or a diabetic ulcer, a pressure sore, a burn or an iatrogenic grating wound. The composition is particularly useful for treating recalcitrant wounds, i.e. wounds which have not healed within three months using standard treatment.

10 The term "single-layered" indicates that the composition has only one layer containing cells within a support matrix, i.e. it is not a multi-layered "skin equivalent" with multiple layers of (different) cells. However, the invention also encompasses compositions having additional non-cellular layers as well as compositions having stacked layers comprising substantially uniform single  
15 layers.

The composition may be incubated for up to about 96 h, for example up to 72 h, 48 h, 25 h, or 24 h, preferably for 16 h to 24 h. Incubation is preferably *in vitro*, but may also be *in situ* (for example, with the composition applied to a wound).

20 In one embodiment, it has been found by the present inventors that taking cells such as passaged human dermal fibroblasts, casting (or seeding) the cells in a matrix such as a protein-based matrix and then incubating this mixture for up to 96 h, for example, results in a wound healing phenotype that is particularly  
25 beneficial for use in wound healing applications. It has been observed that such cells are predominantly in a proliferative phase in culture (encouraged by low density seeding, avoiding contact inhibition).

30 The present inventors have found that under normal culture conditions, for example, a liquid culture of human dermal fibroblasts incubated in a standard culture medium at 37°C, development of a wound-healing phenotype may typically take 2 to 3 days. However, incubation of such fibroblasts in a suitable

environment such as in a support matrix and/or a wound shortens the development process, so that before 24 hours the cells may have entered or reached the wound-healing phenotype. Thus, incubation of cells in a suitable support matrix and/or wound results in a shorter development time to reach a wound healing phenotype than standard (for example, liquid) culture conditions.

The composition is preferably incubated at a temperature of about 37°C. If incubation takes place at a lower temperature, the living cells will develop at a slower rate and incubation time may need to be extended.

Preferably, the composition excludes mitotically inactivated cells (for example cells mitotically inactivated by administration of mitomycin C or other chemically-based mitotic inhibitors, irradiation with  $\gamma$ -rays, irradiation with X-rays, or irradiation with UV light, as described for example in US2003/0165482).

The composition may be stored after incubation (i.e. have a shelf-life) for up to about 40 days, preferably up to 28 days or 21 days or 19 days, and more preferably about 7 to 14 days or about 7 to 11 days at a temperature of 2°C to 8°C, for example 3°C to 5°C, preferably about 4°C, while retaining an ability to heal wounds. The composition therefore does not require freezing, as do certain prior art wound healing compositions. The present composition preferably does not contain a substance added as a cryopreservant or cryoprotectant (such as glycerol and/or human serum albumin).

Once the cells of the composition have been incubated to reach or approach a wound healing phenotype phase, the composition can preferably conveniently be stored at approximately 4°C for up to 40 days, and certainly 7 to 14 days, before use without significant loss of viability or change of phenotype. This has significant practical advantages in that it provides not only an efficacious product comprising cells with a wound healing phenotype (for example cells that are optimally suited for secretion of extracellular matrix with minimal

inappropriate fibrinolysis), but also gives a relatively long shelf-life under commonly available standard refrigeration conditions. The ability to ship such products at approximately 4°C also considerably simplifies transportation. Maintaining a cold chain at 2° to 8°C is considerably simpler and cheaper than shipping at -70°C, as is commonly required for live cells.

The cells are preferably mammalian, for example human.

Cells of the present invention may include fibroblasts, keratinocytes, stratum germinativum cells, and combinations or admixtures of such cells. However, in a preferred embodiment, the cells of the composition may substantially exclude keratinocytes. The cells may be isolated from any suitable mammalian source, and preferably are human. The cells are preferably allogeneic, although autologous and/or xenogeneic cells may be used. The cells may be substantially of one type only, for example 90% to 100%, preferably 95% to 99.5%, and more preferably 97.5% to 99% of one type. In a preferred embodiment, the cells are substantially fibroblasts, for example 90% to 100%, preferably 95% to 99.5%, and more preferably 97.5% to 99% fibroblasts. The fibroblasts may be dermal fibroblasts, preferably human dermal fibroblasts. A preferred embodiment comprises allogeneic human foreskin-derived fibroblasts.

As required for manufacture, cells may be thawed, recovered, expanded in culture (for example, for about a week) or until they reach confluence, and resuspended in appropriate volumes and densities as required. Although early passage cells are preferred, later passage cells may also be used. Preferably the cells have undergone less than 20 passages, more preferably less than 15 passages, most preferably less than 10 passages, for example 7 passages. Once defrosted for use in the present invention, the cells may be incubated further as described.

For the purposes of the present invention, day 0 is the day on which the cells are incubated and begin development and they will reach a wound healing

phenotype within the time-frame described above (for example, up to 4 days, or 96 hours, after day 0).

5 The cells may be actively synthetic or able to become actively synthetic rapidly (for example, following storage).

The cells are preferably not proliferating and/or not senescent. Optimally the cells must be in a synthetic phase of development (or maturity), rather than a proliferative or senescent phase. Proliferation may be useful to increase cell  
10 numbers, but delays the important synthesis of extracellular matrix proteins such as collagen types I and III, fibronectin and vitronectin. Cells that have become senescent do not contribute to wound healing and so serve little purpose as such a therapeutic.

15 The cells may be suspended within the matrix, preferably substantially uniformly within the matrix.

The matrix may be protein-based, for example having a protein concentration in the range of about 3 to 12 mg.ml<sup>-1</sup>. For example, the matrix is preferably a  
20 clottable or gelling substance such as fibrin, collagen, fibronectin, vitronectin, alginate, agar, collagen, PVA, hyaluronic acid, modified starches, carrageenans, carob, gelatine, pectin or gelling agent.

The matrix is preferably non-pyrogenic and/or sterile.

25 In a preferred embodiment, the matrix is a fibrin matrix. The fibrin may have a concentration in the composition in the range of 3 to 12 mg.ml<sup>-1</sup>, for example 7 to 12 mg.ml<sup>-1</sup> or 3 to 5 mg.ml<sup>-1</sup>. The fibrin matrix is preferably formed by thrombin-mediated polymerisation of fibrinogen.

30 The matrix is preferably solid or semi-solid. The matrix of the composition is "pre-cast" in the sense that it is provided as a solid or semi-solid form (such as a

gel). The matrix may be insoluble. Most preferably, the cells are cast in the matrix prior to development of a wound healing phenotype.

5 The rate of fibrinolysis occurring within the composition may be a factor taken into account with a fibrin matrix-based composition. As described above, fibrinolysis is a normal part of the wound healing process, by which the fibrin matrix is gradually replaced by other extracellular matrix proteins. If, however, fibrinolysis occurs too early or too rapidly, the wound healing gel is broken down before useful collagen deposition has occurred. Fibroblast expression of  
10 pro-fibrinolytic factors such as urokinase-type plasminogen activator is developmentally regulated and so the phenotype of fibroblasts where included in the composition is relevant if premature fibrinolysis is to be avoided.

15 The wound healing composition may further comprise a protease inhibitor suitable for preventing breakdown of the matrix. The inhibitor may be a serine protease inhibitor, most preferably one or more selected from the list consisting of aprotinin, e-aminocaproic acid and tranexamic acid. Preferably, especially where the concentration of protein is in the range 7 to 12 mg.ml<sup>-1</sup>, the protease inhibitor is aprotinin. Alternatively, especially where the concentration of  
20 protein is in the range 3 to 5 mg.ml<sup>-1</sup>, the protease inhibitor may be tranexamic acid.

The composition may be incubated in a protein-rich environment.

25 Where the composition is sufficiently solid, it may be provided in any suitable shape and size, to suit the wounds it is design to be used with. Preferably, the composition is substantially disk-shaped. The composition may have a thickness of approximately 8 mm or less, preferably 5 mm or less. The thickness of the matrix will normally determine the thickness of the  
30 composition.

The wound healing composition may comprise about 450 to 2500 cells per

mm<sup>2</sup>, about 500 to 1500 cells per mm<sup>2</sup>, about 750 to 2000 cells per mm<sup>2</sup>, or about 900 to 1700 cells per mm<sup>2</sup> such as about 1450 to 1550 cells per mm<sup>2</sup> and preferably about 1500 cells per mm<sup>2</sup>, or for example about 450 to 550 cells per mm<sup>2</sup> and preferably about 500 cells per mm<sup>2</sup>, as measured per unit area. Lower  
5 cell densities than those indicated may result in poor cell viability. Higher cell densities may result in inhibition of extracellular matrix protein synthesis and progression to a senescent cell phenotype. Within the range of cell densities provided above, specific embodiments of the invention have been developed using approximately 500 cells per mm<sup>2</sup> and approximately 1500 cells per mm<sup>2</sup>.

10 In a preferred embodiment, the wound healing composition comprises cells which are human dermal fibroblasts within a sterile, non-pyrogenic fibrin support matrix formed by thrombin-mediated polymerisation of fibrinogen, and in which the composition has been incubated for 16 to 24 h at about 37°C.

15 The composition may be packaged in a container suitable for transporting the composition (for example, while storing the composition) and/or topically applying the composition to a skin surface. The container may comprise a flexible pouch consisting of two sheets of impermeable flexible material  
20 peripherally sealed to provide a means of containment for the composition, the pouch comprising a first internal surface to which the composition is adherent at a level of adhesion more than that between the composition and a second internal surface of the pouch but less than that between the composition and the skin surface, such that in use the pouch may be opened by parting the sheets and  
25 the composition conveniently manipulated and directly applied to the skin surface without further requirement for the composition to be touched directly by any other means prior to application. For example, the container may be an Oliver (RTM) Products Company "Solvent Resistant Peelable Pouching Material" (Product number Q15/48BF1).

30 In a further aspect of the invention there is provided a wound healing composition as described herein for use as a medicament. For example, the

composition may be for use as a medicament in the treatment of a skin lesion. The composition as a medicament may be used for topical application to a skin lesion or wound as described herein.

- 5 In a further aspect of the invention there is provided a method of manufacturing a wound healing composition as defined herein, comprising the steps of:  
suspending living cells in a solution comprising a polymerisation agent and/or a monomer capable of being polymerised by the polymerisation agent into a matrix;  
10 forming a single-layered support matrix comprising the cells by polymerisation of the monomer with the polymerisation agent; and  
incubating the matrix under conditions (for example, conditions as defined herein, such as temperature and time conditions) which allow development of a wound healing phenotype in the cells, thereby forming a wound healing  
15 composition.

- Where for example the composition comprises monomer without polymerisation agent or polymerisation agent without monomer, the matrix may be formed by adding monomer or polymerisation agent as required to the  
20 solution such that both monomer and polymerisation agent are present in sufficient concentrations to effect polymerisation.

- In another aspect of the invention there is provided a method of manufacturing a wound healing composition as defined herein, comprising the steps of forming a  
25 single-layered support matrix by polymerising a polymerisable monomer with a polymerisation agent, casting living cells into the support matrix, and  
incubating the matrix under conditions (for example, conditions as defined herein, such as temperature and time conditions) which allow development of a wound healing phenotype in the cells, thereby forming a wound healing  
30 composition.

Also provided is a method of manufacturing a wound healing composition,

preferably a wound healing composition as described herein, comprising the steps of suspending living mammalian cells in a solution comprising a protein monomer capable of polymerisation into an insoluble matrix, adding an agent capable of promoting such polymerisation (i.e. a polymerisation agent) and  
5 allowing polymerisation to occur in a mould such that the solid polymerised composition may be removed from the mould and packaged ready for topical administration to a patient. The cells are preferably as described herein.

The monomer may be fibrinogen and the polymerisation agent may be  
10 thrombin. Alternatively, the polymerisation agent may be vitamin K-dependent clotting factors, venom serine proteases (for example, Crotalax, Batroxobin, Gabonase, Okinaxobin, Reptilase, Calobin and Fibrozyne) or other agents with thrombin-like fibrinogen cleaving activity.

15 The cells may have a wound healing phenotype as described herein prior to being suspended in the monomer, or may adopt or develop into such a phenotype during incubation within the time-frames described herein (for example, within 0 h to 96 h after suspension).

20 Polymerisation may occur in a mould.

The methods may include steps adding additional components as described herein to the composition.

25 The method of the invention may comprise the further step of packaging the wound healing composition into a container for storing the composition and/or for transporting the composition and/or for topically applying the composition to a skin surface of a patient.

30 In a further aspect of the invention there is provided the use of living cells as defined herein in the manufacture of a wound healing composition as defined herein for the treatment of a skin lesion.



The invention also provides a method of treating a patient suffering from a skin lesion comprising topically applying of a wound healing composition as defined herein to the skin lesion.

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In a further aspect, the invention provides a container (or package) for a solid or semi-solid, sterile, topical composition (preferably a wound healing composition as described herein) comprising a flexible pouch consisting of two sheets of impermeable flexible material peripherally sealed to provide a means of containment for the composition, the pouch comprising a first internal surface to which the composition is adherent at a level of adhesion more than that between the composition and a second internal surface of the pouch but less than that between the composition and a bodily surface to be treated, such that in use the pouch may be opened by parting said sheets and the composition conveniently manipulated and directly applied to the bodily surface without any requirement for the medicament to be directly touched by any other means before application. The container *per se* aspect of the invention may exclude the Oliver (RTM) Products Company "Solvent Resistant Peelable Pouching Material" (Product number Q15/48BF1).

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In a further aspect, there is provided use of a container as described herein for storing, transporting and/or applying a solid or semi-solid, sterile, topical composition (preferably a wound healing composition as described herein).

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The container provides a convenient means of storage, delivery and application of any form of solid or, especially, semi-solid, materials, especially those intended for topical application to bodily surfaces. Preferably such materials are of a semi-solid or gel nature, such that physical manipulation would without the container be difficult. The preferential adherence of the material to an element of the container, with the ease of transfer thereafter to the skin or other bodily surface, provides a considerable advantage. In particular, such materials may be cut to the required size before application to the intended area. In the case of

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wound healing compositions as herein described, this is a particular advantage.

In a preferred embodiment, the container comprises metal foil, laminated or metalised plastic. In one preferred embodiment it comprises a transparent area  
5 allowing visual inspection of its contents.

Preferably, the internal surfaces of the container and its contents are sterile.

In a preferred embodiment, the first internal surface of the pouch is modified to  
10 increase the adherence of the composition thereto. In one embodiment this comprises application of a coating to the first internal surface. Preferably the coating is selected from the list consisting of: a polymer, a thermoplastic, a thermo-setting plastic, a protein, an amino acid, a carbohydrate.

15 Alternatively, the first internal surface is modified by roughening to increase the adherence of the composition thereto. As used herein, the term "roughening" includes any physical modification of the surface intended to improve adherence, such as embossing, scratching, abrading or scuffing, or chemical roughening by means of etching, erosion, acid or alkali treatment. Other means  
20 of modifying the surface energy properties of the surface in order to improve or modulate the degree of adherence of the solid or semi-solid product are disclosed. Such means include coating the first internal surface of the pouch. Preferably such a coating is selected from the list consisting of a polymer, thermoplastic, thermo-setting plastic, protein, amino acid or carbohydrate.

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In one particularly preferred embodiment, the first internal surface is modified by means of a discontinuous coating, in the form of raised areas or dots, having the effect of providing a roughened surface.

30 Also provided according to the present invention is a method of packaging a sterile, solid or semi-solid topical composition as described herein comprising the step of placing the composition in a container pouch as described herein.

Specific examples of the invention will now be described with reference to the accompanying figures, in which:

5     **Figure 1** is a flow chart summarising a process of manufacturing a wound healing composition according to preferred embodiments of the invention; and

**Figure 2** shows the packaging, manipulation and application of a preferred wound healing composition produced according to a process shown in Fig. 1.  
10     **A:** shows a matrix (or set gel) preferentially adhering to a modified internal surface of one of two metalised plastic sheets of a container pouch. **B:** shows the use of one of the sheets of the container to apply the gel of the wound healing composition to skin. Note that the sheet may used to support the gel while both are cut to the appropriate shape and size. **C:** shows the wound  
15     healing composition in place.

The process of manufacturing preferred compositions of the invention is summarised in Fig. 1. Alternative components or methods as described above may be used in place of those described here.

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In principle, the composition comprises two components, which are cast together. The first component comprises a solution of fibrinogen together with one or more protease inhibitors to prevent unwanted proteolysis by protease contaminants and premature matrix breakdown by cells during storage. In  
25     particular, contaminants may include the naturally fibrinolytic enzyme plasmin, or its precursor plasminogen. Serine protease inhibitors such as aprotinin, e-aminocaproic acid, or its analogue tranexamic acid, are frequently used in order to inhibit plasmin or prevent its activation. Added to this fibrinogen solution is a suspension of living cells in a suitable medium or buffer solution (a “working  
30     cell suspension”).

The second component comprises a solution of thrombin (an enzyme that

naturally acts upon fibrinogen), calcium ions (a required cofactor), and a medium suitable for the culture of living cells. A further clotting factor, Factor XIII, is also activated by thrombin in the presence of calcium ions. Activated Factor XIII promotes polymerisation of monomeric fibrin (cleaved from fibrinogen by thrombin) into a three-dimensional protein insoluble scaffold.

In order to cast a gel (i.e. a matrix in the form of a gel), these two components are combined and, whilst still liquid, poured into a pre-coated suitable mould. Although commonly circular, the gels may be cast into any desired shape. For some applications, other shapes may be more suitable. In particular, essentially or substantially rectangular or elliptical gels may be more convenient for larger wounds.

Enzymatic cleavage of fibrinogen into fibrin monomers and polymerisation of these monomers results in setting of the liquid into a semi-solid gel in which living cells are suspended. For many applications, this gel is then maintained for a period of about 24 hours under suitable conditions for cell growth, division and secretion of extracellular matrix proteins, and other proteins such as growth factors. Following development (or maturation), the cast gel is removed from the casting mould and placed directly into a sterile package (which term is taken herein to have the same meaning as "container"). A small amount of medium, for example a buffer medium, is added to each package to maintain the product during storage and shipping, and the packages are sealed. During storage and shipping the packages are maintained at a temperature of 2°C to 8°C.

In two preferred embodiments, called Protoderm 500 and Protoderm 1500, the composition comprises cells at a density of about 500 cells per mm<sup>2</sup> and about 1500 cells per mm<sup>2</sup>, respectively.

Advantages of such a product over the currently available alternatives include the following. The use of a protein sealant as a scaffold or support matrix allows convenient topical delivery of cells to the wound. The pre-cast gel allows

convenient and accurate application of regenerative cells to the wound surface with control of the distribution and density of cells applied. Manufacture and shipping of other tissue equivalents may take approximately 3 weeks for the matrix alone, whereas the product of the present invention may be  
5 manufactured within 10 days, or even as little as 2 days if sufficient growing cells are available. These factors combine to give cost advantages, so manufacture and production is more cost effective than many other commercially available products.

10 As described below, the product of the invention when packaged also features a unique flat pack system (adhesive backing) ensuring maintenance of product during shipping and “ease of use” of final product. The precast gels can be shipped and stored for up to 28 days at 2 to 8°C, whereas other available products must either be frozen or shipped at room temperature.

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**Example 1: High protein concentration product (‘Protoderm 500’ and ‘Protoderm 1500’)**

A first embodiment of the invention is designed to optimise both rapid  
20 manufacturing of the wound healing product and rapid wound healing by containing cells and protein components at relatively high concentrations.

**Matrix**

In the first embodiment, the matrix protein is fibrin, derived from a commercial  
25 fibrinogen product, Tisseel [RTM] (Baxter). When reconstituted, this provides a convenient two component system to which cells may be added. Components of the matrix are summarised in Table 1. It should be noted that Tisseel [RTM] also contains Factor XIII, as well as plasmafibrinectin and plasminogen.

30 **Table 1 – Primary components of Tisseel [RTM]**

Component	Final concentration in cellularised scaffolds
Matrix protein (fibrinogen)	7.5 - 11.5 mg/ml
Aprotinin	300 K IU/ml
Thrombin	25 IU/ml
Calcium chloride	4 mM

As will be apparent to one of appropriate skill in the art, the concentrations of these components can be varied as required. For example, fibrinogen may be used in concentrations of the approximate range  $7\text{--}20\text{mg.ml}^{-1}$  for this application, thrombin in the range 5-50 IU/ml (in fact, trace levels of contaminating thrombin may lead eventually to fibrin formation and gel setting without additional thrombin, but this is inconvenient and unpredictable), and calcium chloride in the range 2–20mM. Aprotinin is used to prevent unwanted fibrinolysis but, again, the exact concentration may be varied.

10

### Cells

Human dermal fibroblasts were obtained by culture of cells derived from neonatal foreskin tissue. Under GMP (Good Manufacturing Practice) conditions, fibroblastic cells were isolated by collagenase digestion and expanded by culture and serial passage according to routine laboratory practice to establish a master cell bank (MCB). The MCB was screened against a panel of human and animal-derived viruses, bacteria, mycoplasma and fungi, and for tumorigenicity by a GLP (Good Laboratory Practice)-accredited facility and determined to be free of contamination. Several working cell banks (WCB) were then established for manufacture of the product, rescreened and stocks of cells frozen according to standard procedures.

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It is also envisaged that for various patient-specific applications, autologous

fibroblasts or other cells obtained from biopsies may be cultured and expanded for use.

5 The cells were suspended in the quantities shown below (P-500 refers to Protoderm-500; P-1500 refers to Protoderm-1500) in Liebowitz L-15 cell culture medium buffered and supplemented as shown in Table 2 before addition to the fibrinogen component. As will be apparent to one of skill in the art, medium not intended for use in a CO<sub>2</sub>-enriched atmosphere (commonly used in tissue culture incubators or sealed flasks) must be appropriately buffered by  
10 some other system. Such media, supplemented with, for instance, HEPES, are well-known in the art. Liebowitz L-15 medium relies on a phosphate buffering system. The medium was supplemented with sodium bicarbonate and dextrose, as shown.

15 For convenience and consistency, a standard 'working cell suspension' of  $1.5 \times 10^6$  cells.ml<sup>-1</sup> was generally prepared.

#### Preparation of fibrin sealant

20 As outlined in Fig. 1 and summarised below, Tisseel [RTM] thrombin powder was reconstituted in a calcium chloride solution according to the manufacturer's directions.

Once dissolved, the Thrombin/CaCl<sub>2</sub> solution was further diluted with supplemented L-15 medium to obtain a 'Working Thrombin Solution' and  
25 refrigerated until further use for a minimum of 15 minutes. (Gels may also be manufactured with 'Working Thrombin Solution' at room temperature.) Freeze-dried fibrinogen was reconstituted with an aprotinin solution before being added to the working cell suspension in supplemented L-15 medium. Once reconstituted, the fibrinogen should be used within 4 h, ideally within 1 to 2 h.

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Working thrombin solution (6.75 ml) contains:

Thrombin: 50IU/ml (or 337.5IU total)

Calcium chloride: 8 $\mu$ moles/ml (or 54  $\mu$ moles total)

In supplemented L-15

(Total refers to the amount in 6.75mls)

5 Working fibrinogen and cell suspension mix (total volume 6.75ml):

Tisseel: 19mg/ml (or 128.25mg total)

Aprotinin: 600KIU/ml (or 4050KIU total)

Cells: 1.2x10<sup>6</sup> cell/ml (8.1x10<sup>6</sup> cells total for P-1500); or

0.4x10<sup>6</sup> cell/ml (2.7x10<sup>6</sup> cells total for P-500)

10 in supplemented L-15

(Total refers to the amount in 6.75mls)

**Table 2 - Details of Medium Used for Example 1**

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<b>Components (Supplier shown in parentheses)</b>	<b>Function</b>	<b>Concentration per ml</b>
L-15 medium (Cambrex)	Nutrient delivery to the cellular component of the product. Maintains cell viability and structure of the gel.	N/A (base medium)
Sodium Bicarbonate (Mallinckrodt Chemical)	Required for cell viability	202.5 $\mu$ g
Dextrose (J.T. Baker)	Nutrient	4.5mg
Adenine (ABCR)	Base required for cell viability	24.4 $\mu$ g
L-Glutamine (Molekula)	Amino acid for cell viability	0.29mg



Ethanolamine (Molekula)	Phospholipid for cell metabolism	6.2 $\mu$ g
O-phosphoryl- ethanolamine (Merck)	Phospholipid for cell metabolism	14.12 $\mu$ g
Hydrocortisone (Spectrum Laboratory Products, Inc.)	Steroid required for cell metabolism	0.4mg
Human Recombinant Insulin (Serologicals)	Essential hormone	5 $\mu$ g
Selenious acid (Molekula)	Trace substrate for metabolism	6.78ng
3,3',5-Triiodo-L- thyronine (ABCR)	Hormone	1.35ng
apo-Transferrin, bovine (Serologicals)	Cofactor for iron metabolism	5 $\mu$ g
Gamma Irradiated Foetal Bovine serum or New Born calf serum (JRH or Hyclone)	Nutrients	2%v/v

Note: As will be apparent to one of ordinary skill in the art, sources of ingredients used to producing the wound healing composition may differ depending on the grade or purity required for different applications. For example, for clinical applications of the product, pharmaceutical grade materials may be required.

### Casting the gels

The working thrombin solution (6.75ml) and Tisseel [RTM] fibrinogen/cell suspension mixture (6.75ml) were combined by means of a Duplojet mixer unit and loaded into a suitable pre-coated casting container (conveniently a sterile Petri dish or similar) via a 16G needle or equivalent. It is useful to pre-coat the casting dish with serum containing media or albumin to prevent the gel from adhering. The gel set within a few minutes. The gel was then bathed in 20ml of medium (Table 2) and the casting dish covered with a lid. The set gel was incubated at 37°C for 16–24 hours to allow development (or maturation) of the cells.

### Packing and Storage

After development (or maturation), the set gels were removed from their casting containers and placed into pre-irradiated, sterile foil pouches, stored within a sterile roto-seal bag. 10ml serum-free medium (as per Table 2, without the foetal bovine serum) was added to each pouch before sealing. The shelf life of the sealed units is up to 28 days at 4°C.

### Example 2: Low protein concentration product

For certain applications, it is possible to use lower protein concentrations. The chief advantage of this is reduction of production costs, since serum-derived proteins and many protease inhibitors, such as aprotinin, are expensive. In a preferred embodiment, the concentration of fibrin in the set product is reduced to less than 7 mg.ml<sup>-1</sup>. In practice, 3.0–4.0 mg.ml<sup>-1</sup> is found to be effective.

One important consideration is the effectiveness (as well as the cost) of using aprotinin as protease inhibitor in such 'low protein' products. In particular, *pro rata* dilution of commercial products results in aprotinin concentrations that are too low to be effective. A preferable solution is to use an alternative inhibitor, such as tranexamic acid. Not only is this a highly effective inhibitor of

fibrinolysis, but it has significant cost advantages.

### Matrix

In this embodiment the matrix protein is fibrin, sourced from a commercial fibrin sealant, Tisseel [RTM], using tranexamic acid instead of aprotinin. The key components of the matrix are summarised in Table 3. It should be noted that the same matrix composition could also be achieved using another commercially available fibrin sealant, Quixil. However the addition of exogenous tranexamic acid should be reduced as it already contains this inhibitor.

**Table 3 - Components of the Fibrinogen Matrix in Example 2**

<b>Component</b>	<b>Final concentration in cellularised scaffolds</b>
Matrix protein (fibrinogen)	3.5mg/ml
Tranexamic acid	10mg/ml
Thrombin	25IU/ml
Calcium chloride	4mM

Freeze-dried Tisseel [RTM] fibrinogen is reconstituted with supplemented L-15 medium solution before being added to the working cell suspension in supplemented L-15 medium. Once reconstituted, Tisseel [RTM] fibrinogen should be used within 4 hours, ideally within 1-2 hours.

Tisseel [RTM] thrombin powder is reconstituted in a calcium chloride solution according to the manufacturer's directions. Once dissolved, the thrombin/CaCl<sub>2</sub> solution is further diluted with supplemented L-15 medium containing tranexamic acid to obtain a working thrombin solution.

The cell density used is again in the range 450 to 2500 cells mm<sup>-2</sup>. In order to minimise costs, it may be desirable to use a cell density of approximately 450 to

550 cells  $\text{mm}^{-2}$ . It should be noted, however, that protein concentration and cells density are independent variables. Lowering protein concentration is the major cost determinant, rather than cell density. However, being able to use fewer cells may have implications for the speed of production. In any case, high cell density/low protein concentration and low cell density/high protein concentration embodiments are envisaged and may be preferred in specific circumstances.

### **Example 3: Packaging, storage and delivery**

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A major factor contributing to the success of topical wound healing compositions is the ease of accurately applying them to the wound surface so that a close contact is established, without air bubbles or creases, under sterile operating conditions. Wound healing compositions may be fragile, and handling should be kept to a minimum. The composition of the invention is preferably packaged in such a way as to significantly assist and facilitate application. In addition, the composition is shipped and stored chilled, rather than frozen, so that detailed thawing procedures are not required prior to use.

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After setting and the 16–24 hour culture and development (or maturation) period, the individual gel discs are packaged by insertion into a flexible foil or metalised plastic pouch comprising two rectangular sheets, sealed along a substantial portion of three of their sides so as to form an open pocket. The inner surface of one of these sheets is modified so as to increase its adherence to the gel product. In a preferred embodiment as shown in Fig. 2, the packaging used is an Oliver [RTM] Products Company (Grand Rapids, Michigan USA) peelable foil pouch comprising one foil sheet and one sheet of laminated polyester/foil sheet with Q15 Adhesive dot pattern coating. Q15/48BF1 is a laminated lidding and pouching material for medical devices. The purpose of this dot pattern adhesive coating is to improve the efficiency of the heat sealing process which is used to seal the edges of the sheets together. However, the adhesive and raised dot pattern prove highly effective in providing a surface to

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which composition preferentially adheres, as compared with the smooth, uncoated inner surface of the opposing sheet. Other forms of coating and/or roughening of the surface of one of the internal surfaces of the pouch could be used to achieve the same effect. Similarly, any suitably durable, flexible, water and gas-impermeable sheet material might be used to manufacture such a pouch. All or part of the packaging might be transparent to allow visual inspection, for example, of the integrity of the composition or of the colour of a pH indicator dye in the cell culture medium, a small volume of which is inserted in the pouch, along with the composition, before the pouch is sealed along its remaining open edge.

Thus sealed, the composition has a shelf-life of at least 7–11 days, and preferably up to 28 days, more preferably 21 days, at 2° to 8°C.

For application, as shown in Fig. 2, the pouch is peeled apart, under sterile conditions, leaving the composition adhering to the treated inner surface of one of the sheets comprising the pouch. Using the sheet as a backing or means of support the composition is then applied to the surface of the wound, to which, in the absence of excessive exudation, it will preferentially adhere allowing it to be peeled away from the sheet. This means of application allows the composition to be applied without wrinkling or incorporation of air bubbles, and with the minimum of manipulation. The edges of the composition may be easily trimmed to fit the limits of the wound. Another advantage of delivering the composition in a format that is reversibly adherent to the packaging, as described, is that it allows the easy identification of the orientation of the product and facilitates oriented application, should this be required. In the case of a homogenous wound-healing product, orientation of the product on the wound is not important. However, where a multilayered composition is involved, such as one with a fibroblast layer that is intended to be applied in contact with the wound surface and a keratinocyte layer that is intended to be oriented away from the wound surface, it may be difficult or impossible to establish the orientation visually. In this case, the ability to deliver the product

in such a way as makes incorrect application impossible without first removing the composition from the packaging offers a significant advantage.

5 The foregoing examples are meant to illustrate the invention and do not limit it in any way. One of skill in the art will recognise modifications within the spirit and scope of the invention as indicated in the claims.

All references cited herein are hereby incorporated by reference.